



US009047695B2

(12) **United States Patent**
Tseng et al.

(10) **Patent No.:** **US 9,047,695 B2**
(45) **Date of Patent:** **Jun. 2, 2015**

(54) **TRANSFORMATION METHOD FOR
DIFFUSION SPECTRUM IMAGING USING
LARGE DEFORMATION Diffeomorphic
METRIC MAPPING**

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(*) Notice: Subject to any disclaimer, the term of this
patent is extended or adjusted under 35
U.S.C. 154(b) by 289 days.

(21) Appl. No.: **13/644,211**

(22) Filed: **Oct. 3, 2012**

(65) **Prior Publication Data**
US 2014/0044332 A1 Feb. 13, 2014

(30) **Foreign Application Priority Data**
Aug. 10, 2012 (TW) 101129000 A

(51) **Int. Cl.**
G06K 9/00 (2006.01)
G06T 11/00 (2006.01)
G06T 7/00 (2006.01)

(52) **U.S. Cl.**
CPC **G06T 11/003** (2013.01); **G06T 7/0014**
(2013.01); **G06T 7/003** (2013.01); **G06T**
7/0044 (2013.01); **G06T 2207/10088** (2013.01);
G06T 2207/20076 (2013.01); **G06T 2207/30016**
(2013.01)

(58) **Field of Classification Search**
None
See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

4,292,124	A *	9/1981	Fisch	376/132
6,549,803	B1 *	4/2003	Raghavan et al.	600/431
6,940,664	B1 *	9/2005	Pilu	359/806
7,230,429	B1 *	6/2007	Huang et al.	324/322
7,423,430	B1 *	9/2008	Sharif et al.	324/309
7,505,806	B2 *	3/2009	Masutani et al.	600/410
7,689,017	B2 *	3/2010	Karl et al.	382/128
7,970,194	B2 *	6/2011	Kimura	382/131
8,031,927	B2 *	10/2011	Karl et al.	382/131
8,094,904	B2 *	1/2012	Slabaugh et al.	382/130
8,111,893	B2 *	2/2012	Chen et al.	382/131
8,170,305	B2 *	5/2012	Laidlaw et al.	382/128
8,170,644	B2 *	5/2012	Du	600/416
8,502,534	B2 *	8/2013	Lai et al.	324/309
8,577,112	B2 *	11/2013	Mori et al.	382/131
2002/0042569	A1 *	4/2002	Wedeen	600/411
2004/0120565	A1 *	6/2004	Wollenweber	382/131
2004/0161141	A1 *	8/2004	Dewaele	382/132
2004/0197015	A1 *	10/2004	Fan et al.	382/128

(Continued)

OTHER PUBLICATIONS

Google Scholar NPL Search—Sep. 5, 2014, pp. 1-2.*

(Continued)

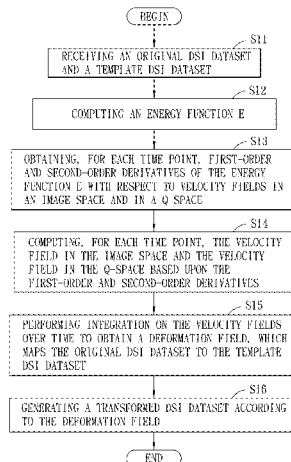
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(57) **ABSTRACT**

A transformation method for diffusion spectrum imaging includes: receiving an original DSI dataset and a template DSI dataset; computing an energy function; computing, for each time point, first-order and second-order derivatives of the energy function with respect to velocity fields in an image space and in a q-space; computing, for each time point, the velocity fields in the image space and in the q-space based upon the first-order and second-order derivatives; performing integration on the velocity fields over time to obtain a deformation field; and generating a transformed DSI dataset according to the deformation field.

6 Claims, 3 Drawing Sheets



(56)

References Cited

U.S. PATENT DOCUMENTS

2006/0094951	A1 *	5/2006	Dean et al.	600/407
2006/0158447	A1 *	7/2006	McGraw et al.	345/419
2007/0014457	A1 *	1/2007	Jolly et al.	382/128
2007/0092120	A1 *	4/2007	Guo et al.	382/128
2007/0092122	A1 *	4/2007	Xiao et al.	382/128
2007/0265518	A1 *	11/2007	Boese et al.	600/407
2008/0051648	A1 *	2/2008	Suri et al.	600/407
2008/0118132	A1 *	5/2008	Ubelhart et al.	382/131
2008/0247622	A1 *	10/2008	Aylward et al.	382/131
2008/0278804	A1 *	11/2008	Gharib et al.	359/462
2008/0292163	A1 *	11/2008	DiBella et al.	382/131
2009/0003655	A1 *	1/2009	Wollenweber	382/107
2009/0041188	A1 *	2/2009	Keall et al.	378/65
2009/0074276	A1 *	3/2009	Doi et al.	382/130
2009/0096454	A1 *	4/2009	Reisman	324/320
2009/0284257	A1 *	11/2009	Bammer et al.	324/307
2009/0299154	A1 *	12/2009	Segman	600/301
2009/0304248	A1 *	12/2009	Zalis et al.	382/131
2010/0004526	A1 *	1/2010	Wei et al.	600/407
2010/0056897	A1 *	3/2010	Zhang	600/407
2010/0127703	A1 *	5/2010	Sung et al.	324/309
2010/0239141	A1 *	9/2010	Rouet et al.	382/131
2010/0239144	A1 *	9/2010	Fichtinger et al.	382/131
2010/0284595	A1	11/2010	Mori et al.	
2010/0308821	A1 *	12/2010	Poupon et al.	324/309
2011/0092794	A1 *	4/2011	Miller et al.	600/407
2011/0103672	A1 *	5/2011	Miller et al.	382/131

2011/0142316	A1 *	6/2011	Wang et al.	382/131
2011/0245650	A1 *	10/2011	Kerwin et al.	600/407
2011/0274330	A1 *	11/2011	Mori et al.	382/131
2012/0078085	A1 *	3/2012	Xue et al.	600/420
2013/0030757	A1 *	1/2013	Stotzka et al.	702/156
2013/0182932	A1 *	7/2013	Chen et al.	382/131
2013/0195335	A1 *	8/2013	Gorman et al.	382/131
2013/0231548	A1 *	9/2013	Brown et al.	600/407
2013/0259340	A1 *	10/2013	Tseng et al.	382/131

OTHER PUBLICATIONS

Leventon et al. "Statistical Shape Influence in Geodesic Active Contours" Computer Vision and Pattern Recognition, Jun. 2000, pp. 1-8 IEEE.*

Zhukov et al. "Heart-Muscle Fiber Reconstruction from Diffusion Tensor MRI" IEEE Visualization 2003, Oct. 19-24, 2003, Seattle, Washington, USA.*

Ashburner, John. "A fast diffeomorphic image registration algorithm" NeuroImage 38 (2007) 95-113.*

Chumchob et al. "A Robust Affine Image Registration Method" International Journal Of Numerical Analysis and Modeling, vol. 6, No. 2, pp. 1-24.*

Pannek et al. "HOMOR: Higher Order Model Outlier Rejection for high b-value MR diffusion data" Neuroimage 63 (2012) pp. 1-8 (835-842).*

Christensen et al. "Consistent Image Registration" IEEE Transactions On Medical Imaging, vol. 20, No. 7, Jul. 2001, pp. 1-15.*

* cited by examiner

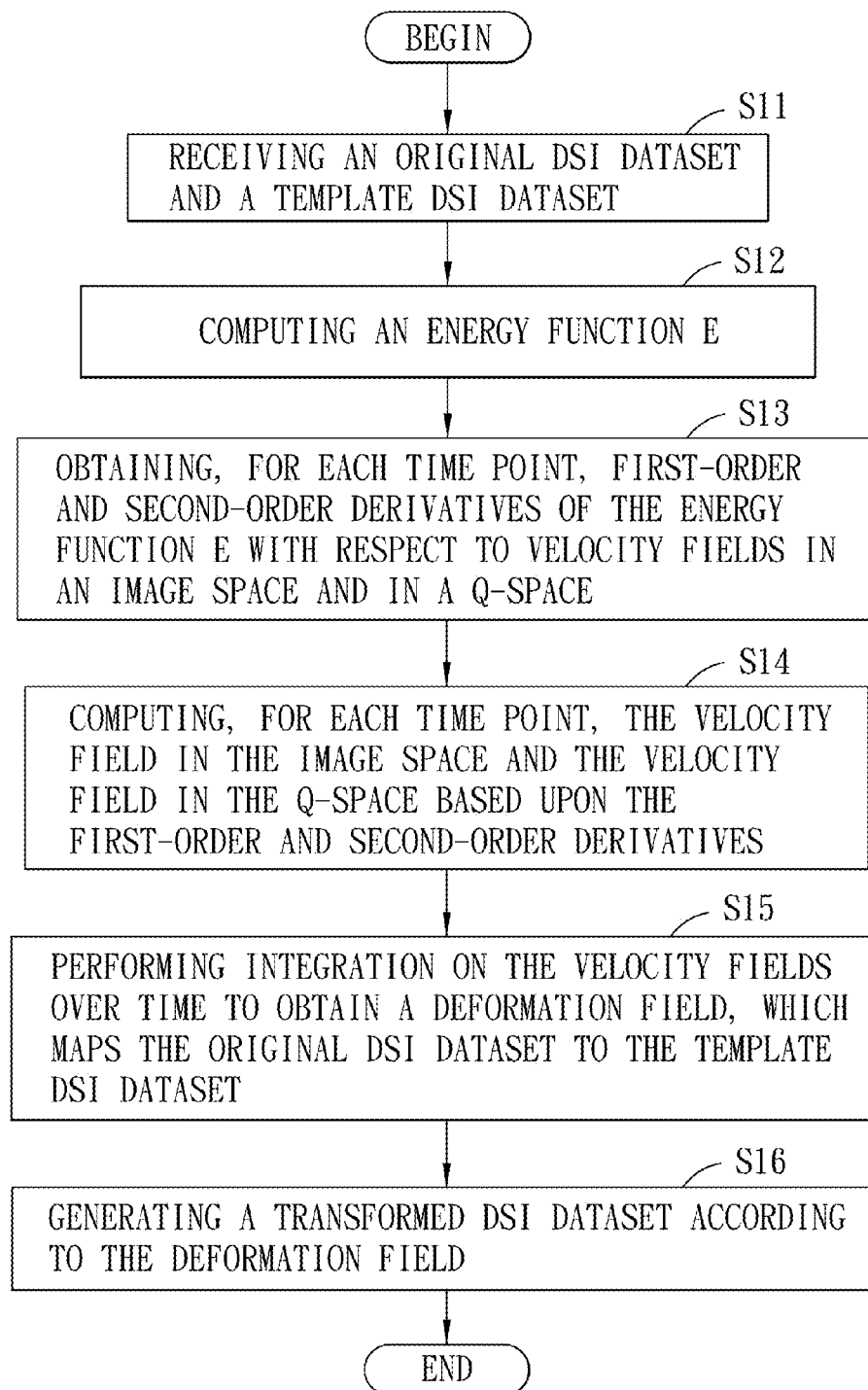


FIG. 1

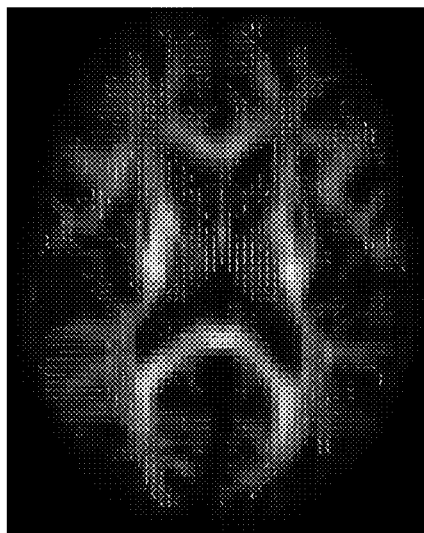


FIG. 2

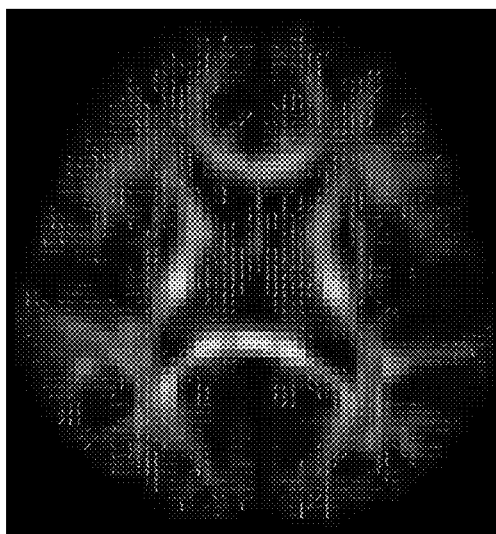


FIG. 3

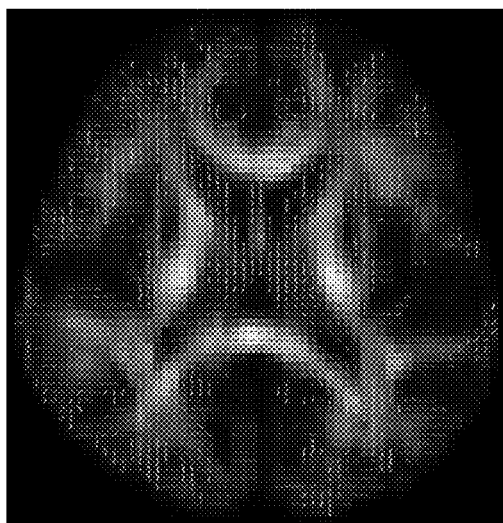


FIG. 4

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TRANSFORMATION METHOD FOR DIFFUSION SPECTRUM IMAGING USING LARGE DEFORMATION DIFEOMORPHIC METRIC MAPPING

CROSS-REFERENCE TO RELATED APPLICATION

This application claims priority to Taiwanese Application No. 101129000, filed on Aug. 10, 2012.

BACKGROUND OF THE INVENTION

1. Field of the Invention

The invention relates to an image processing method, and more particularly to an image processing method for magnetic resonance imaging.

2. Description of the Related Art

Diffusion MRI is a non-invasive imaging method suitable for evaluating fiber orientation of a specific region and revealing the underlying white matter structure of the human brain. One of the approaches is the diffusion tensor imaging (DTI), where the water diffusion is modelled as Gaussian distribution. Practically, a DTI dataset consists of six diffusion weighted (DW) images by applying the diffusion-sensitive gradients in six non-collinear directions, and one null image with no application of diffusion-sensitive gradient. The water diffusion is encoded in the signal intensity of the DW images. Therefore, with appropriate processing on the signal intensity of the DTI dataset, the diffusion tensor in each voxel can be estimated. The diffusion tensor could be represented by a symmetric 3-by-3 matrix, where the principal eigenvector of the matrix is usually assumed to coincide with the underlying fiber orientation. The fiber orientation map can be further processed to reconstruct the fiber pathways.

However, the Gaussian assumption limits DTI to detect at most one fiber orientation in each voxel. Consequently, in regions with crossing fibers, it is difficult for DTI to resolve the fiber orientations and would lead to inaccurate estimation of the anisotropy index.

The crossing fiber problem could be resolved through estimating the diffusion orientation distribution function (ODF). The diffusion ODF could be estimated by the high angular resolution diffusion image (HARDI) methods, such as q-ball imaging (QBI), or by a grid sampling scheme, which is also called diffusion spectrum imaging (DSI). All of the methods do not impose any diffusion models.

In neuroimage studies, it is usually required to transform the brain images to a common space, the so-called template space, to perform the analyses (e.g., statistical comparisons between healthy and patient groups). It is known in the art to use a linear or non-linear method to transform a three-dimensional (3D) brain image to the template space. However, the conventional 3D transformation methods can only deal with scalar images. For an appropriate transformation on diffusion images such as DTI, QBI or DSI, not only the anatomical structures need to be registered, but the diffusion profiles require to be aligned.

SUMMARY OF THE INVENTION

Therefore, an object of the present invention is to provide a transformation method that may completely transform image spatial information and diffusion information for diffusion spectrum imaging (DSI) datasets.

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According to the present invention, a transformation method for DSI comprises:

a) receiving an original DSI dataset and a template DSI dataset;

5 b) using a processor to compute an energy function E;

c) using the processor to obtain, for each time point, a first-order derivative and a second-order derivative of the energy function E computed in step b) with respect to velocity field in an image space and a first-order derivative and a second-order derivative of the energy function E computed in step b) with respect to velocity field in a q-space;

d) using the processor to compute, for each time point, the velocity field in the image space and the velocity field in the q-space based upon the first-order and second-order derivatives obtained in step c);

e) using the processor to perform integration on the velocity fields obtained in step d) over time to obtain a deformation field, which maps the original DSI dataset to the template DSI dataset; and

f) using the processor to generate a transformed DSI dataset according to the deformation field obtained in step e).

BRIEF DESCRIPTION OF THE DRAWINGS

Other features and advantages of the present invention will become apparent in the following detailed description of the preferred embodiment with reference to the accompanying drawings, of which:

FIG. 1 is a flow chart illustrating steps of a preferred embodiment of the transformation method for diffusion spectrum imaging (DSI) according to the present invention;

FIG. 2 is an image of an original DSI of an example;

FIG. 3 is an image of the template DSI of the example; and

FIG. 4 is an image transformed using the preferred embodiment of the transformation method.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

Referring to FIG. 1, the preferred embodiment of the transformation method for diffusion spectrum imaging (DSI) according to this invention is implemented by a processor of a computer after the computer loads a proprietary program stored in a storage medium. The transformation method comprises the following steps:

Step S11: Receiving an original DSI dataset (such as the image shown in FIG. 2) and a template DSI dataset (such as the image shown in FIG. 3). A DSI image set often includes hundreds of images, and FIGS. 2 and 3 are obtained by summarizing the hundreds of the images to a generalized fractional anisotropy (GFA) map.

Step 12: Using a processor of the computer to compute an energy function E, which is:

$$E = E_1 + E_2 = \frac{1}{2} \int_0^1 \|v_t\|^2 dt + \frac{1}{2\sigma^2} \int \frac{(W I_0) \cdot g_{10} - W I_1)^2 dq dx}{E_2} \quad (1)$$

where E_1 is an energy of the transformation path, E_2 is an energy representing data-matching, x is a three-dimensional coordinate in an image space, and q is a three-dimensional coordinate in a q-space. v_t is velocity field at time t , σ is a parameter controlling the relative contribution between E_1 and E_2 , W is a predetermined weighting function, I_0 is the template DSI dataset, and I_1 is the original DSI dataset. The

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interpretation of g_{ab} is that for a particle located at (x, q) at time $t=a$, $g_{ab}(x, q)$ is a position of the particle at time $t=b$. Thus, g_{10} could be considered as a deformation mapping function of WI_0 when $t=1$. The weighting function $W(q)$ is to compensate low signal intensity in regions with high $|q|$ values.

Step 13: Using the processor to obtain, for each time point, a first-order derivative and a second-order derivative of the energy function E computed in step 12 with respect to velocity field in the image space and a first-order derivative and a second-order derivative of the energy function E computed in step 12 with respect to velocity field in the q-space.

A large deformation diffeomorphic metric mapping (LD-DMM), which is proposed by Beg, M. F. et al. in 2005, is used in this preferred embodiment. The transformation process is assumed to behave like liquid flow, so that there is an associated velocity field at each time point. In other words, the velocity field is a function of time.

In this embodiment, the first-order derivative of the energy function E with respect to the velocity field in the image space is computed using the following equation (2):

$$\frac{\partial E}{\partial v_{x,t}} = v_{x,t} - K \left[\frac{1}{\sigma^2} \int |Dg_{t,1}| |\nabla_x J_t^0 (J_t^0 - J_t^1) dq| \right] \quad (2)$$

The first-order derivative of the energy function E with respect to the velocity field in the q-space is computed using the following equation (3):

$$\frac{\partial E}{\partial v_{q,t}} = v_{q,t} - K \left[\frac{1}{\sigma^2} |Dg_{t,1}| |\nabla_q J_t^0 (J_t^0 - J_t^1)| \right] \quad (3)$$

where $v_{x,t}$ is the velocity field in the image space at time t , $v_{q,t}$ is the velocity field in the q-space at time t , K is a smoothing operator characterizing the smoothness of the velocity field, $J_t^0 = (WI_0) \circ g_{t0}$, and $J_t^1 = (WI_1) \circ g_{t1}$.

The second-order derivative of the energy function E with respect to the velocity field in the image space is computed using the following equation (4):

$$\frac{\partial^2 E}{\partial v_{x,t}^2} = K \left[\frac{1}{\sigma^2} \int |Dg_{t,1}| |(\nabla_x J_t^0)(\nabla_x J_t^0)^T| dq \right] \quad (4)$$

The second-order derivative of the energy function E with respect to the velocity field in the q-space is computed using the following equation (5):

$$\frac{\partial^2 E}{\partial v_{q,t}^2} = K \left[\frac{1}{\sigma^2} |Dg_{t,1}| |(\nabla_q J_t^0)(\nabla_q J_t^0)^T| \right] \quad (5)$$

Step 14: Using the processor to compute, for each time point, the velocity field in the image space and the velocity field in the q-space based upon the first-order and second-order derivatives obtained in step 13.

In this embodiment, the first-order and second-order derivatives obtained in step 13 are applied to a Levenberg-Marquardt (LM) algorithm to accelerate calculation as in the following equations (6) and (7):

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$$v_{x,t}^{(n+1)} = v_{x,t}^{(n)} - K \left[\left(\frac{1}{\sigma^2} |Dg_{t,1}| |(\nabla_x J_t^0)(\nabla_x J_t^0)^T| + \delta I \right)^{-1} \right. \quad (6)$$

$$\left. \left(K^{-1} v_{x,t}^{(n)} - \frac{1}{\sigma^2} |Dg_{t,1}| |\nabla_x J_t^0 (J_t^0 - J_t^1)| \right) dq \right]$$

$$v_{q,t}^{(n+1)} = v_{q,t}^{(n)} - K \left[\left(\frac{1}{\sigma^2} |Dg_{t,1}| |(\nabla_q J_t^0)(\nabla_q J_t^0)^T| + \delta I \right)^{-1} \right. \quad (7)$$

$$\left. \left(K^{-1} v_{q,t}^{(n)} - \frac{1}{\sigma^2} |Dg_{t,1}| |\nabla_q J_t^0 (J_t^0 - J_t^1)| \right) \right]$$

where K^{-1} is an inverse operator of K . Calculation may converge after about 5 iterations ($n=5$), and the velocity field in the image space and the velocity field in the q-space at time t are thus obtained.

Step 15: Using the processor to perform integration on the velocity fields obtained in step 14 over time to obtain a deformation field which maps the original DSI dataset to the template DSI dataset. The deformation field is obtained according to the following equation (8):

$$\frac{dg_{0t}}{dt} = v_t \circ g_{0t} \quad (8)$$

where \circ denotes function composition. Here the deformation field $g_{0t} = (g_{x,0t}, g_{q,0t})$, where $g_{x,0t}$ which is an image space component of g_{0t} is a function of x , and $g_{q,0t}$ which is a q-space component of g_{0t} is a function of both x and q . Similarly, $v_t = (v_{x,t}, v_{q,t})$, where $v_{x,t}$ which is an image space component of v_t is a function of x , and $v_{q,t}$ which is a q-space component of v_t is a function of both x and q .

Step 16: Using the processor to generate a transformed DSI dataset according to the deformation field obtained in step 15. The transformed DSI dataset is shown as the image in FIG. 4.

It should be noted that the processors used in each step of this method may be the same or different.

To sum up, the transformation method of this invention uses not only the three-dimensional information in the image space, but also the three-dimensional diffusion information of the DSI dataset, in a total of six dimensions. Therefore, when the original DSI dataset is registered to the template space, details like diffusion information in the image space and in the q-space may be completely transformed, so as to enhance precision of the subsequent comparison and application.

While the present invention has been described in connection with what is considered the most practical and preferred embodiment, it is understood that this invention is not limited to the disclosed embodiment but is intended to cover various arrangements included within the spirit and scope of the broadest interpretation so as to encompass all such modifications and equivalent arrangements.

What is claimed is:

1. A transformation method for diffusion spectrum imaging (DSI) comprising:

- a) receiving an original DSI dataset and a template DSI dataset;
- b) using a processor to compute an energy function E ;
- c) using the processor to obtain, for each time point, a first-order derivative and a second-order derivative of the energy function E computed in step b) with respect to velocity field in an image space and a first-order derivative and a second-order derivative of the energy function E computed in step b) with respect to velocity field in a q-space;

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- d) using the processor to compute, for each time point, the velocity field in the image space and the velocity field in the q-space based upon the first-order and second-order derivatives obtained in step c);
- e) using the processor to perform integration on the velocity fields obtained in step d) overtime to obtain a deformation field, which maps the original DSI dataset to the template DSI dataset, wherein the deformation field is calculated according to:

$$\frac{dg_{0t}}{dt} = v_t \circ g_{0t};$$

and

wherein the deformation field $g_{0t} = (g_{x,0t}, g_{q,0t})$, where x is a three-dimensional coordinate in the image space, q is a three-dimensional coordinate in the q-space, $g_{x,0t}$ which is an image space component of g_{0t} , is a function of x , and $g_{q,0t}$ which is a q-space component of g_{0t} , is a function of both x and q ; and the velocity field $v_t = (v_{x,t}, v_{q,t})$ where $v_{x,t}$ which is an image space component of v_t , is a function of x , and $v_{q,t}$ which is a q-space component of v_t , is a function of both x and q ; and

- f) using the processor to generate a transformed DSI dataset according to the deformation field obtained in step e).

2. The transformation method as claimed in claim 1, wherein, in step d), the velocity field for each time point is calculated using an iterative Levenberg-Marquardt algorithm.

3. The transformation method as claimed in claim 1, wherein, in step b), the energy function is:

$$E = E_1 + E_2 = \frac{1}{2} \int_0^1 \|v_t\|^2 dt + \frac{1}{2\sigma^2} \int ((W I_0) \circ g_{10} - W I_1)^2 dq dx \quad (1)$$

where E_1 is an energy of the transformation path, E_2 is an energy representing data-matching, v_t is the velocity field at time t , σ is a parameter controlling the relative contribution between E_1 and E_2 , W is a predetermined weighting function, I_0 is the template DSI dataset, I_1 is the original DSI dataset, g_{10} is a deformation mapping function of $W I_0$ when $t=1$, x is a three-dimensional coordinate in the image space, and q is a three-dimensional coordinate in the q-space.

4. A transformation method for diffusion spectrum imaging (DSI) comprising:

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- a) receiving an original DSI dataset and a template DSI dataset;
- b) using a processor to compute an energy function E :

$$E = E_1 + E_2 = \frac{1}{2} \int_0^1 \|v_t\|^2 dt + \frac{1}{2\sigma^2} \int ((W I_0) \circ g_{10} - W I_1)^2 dq dx \quad (1)$$

where E_1 is an energy of the transformation path, E_2 is an energy representing data-matching, v_t is the velocity field at time t , σ is a parameter controlling the relative contribution between E_1 and E_2 , W is a predetermined weighting function, I_0 is the template DSI dataset, I_1 is the original DSI dataset, g_{10} is a deformation mapping function of $W I_0$ when $t=1$, x is a three-dimensional coordinate in the image space, and q is a three-dimensional coordinate in the q-space;

- c) using the processor to obtain, for each time point, a first-order derivative and a second-order derivative of the energy function E computed in step b) with respect to velocity field in an image space and a first-order derivative and a second-order derivative of the energy function E computed in step b) with respect to velocity field in a q-space;

- d) using the processor to compute, for each time point, the velocity field in the image space and the velocity field in the q-space based upon the first-order and second-order derivatives obtained in step c);

- e) using the processor to perform integration on the velocity fields obtained in step d) overtime to obtain a deformation field, which maps the original DSI dataset to the template DSI dataset;

- f) using the processor to generate a transformed DSI dataset according to the deformation field obtained in step e).

5. The transformation method as claimed in claim 4, wherein, in step e), the deformation field is calculated according to:

$$\frac{dg_{0t}}{dt} = v_t \circ g_{0t};$$

where v_t is velocity field at time t , g_{0t} is the deformation field at time t , and \circ denotes function composition.

6. The transformation method as claimed in claim 4, wherein, in step d), the velocity field for each time point is calculated using an iterative Levenberg-Marquardt algorithm.

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